



Lymphatic system and Nanoparticulate carriers for lymphatic delivery

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Abstract

The lymphatic system consists of lymph, lymphatic pathways such as lymphatic capillary, lymphatic vessel, lymphatic duct etc., and some lymphatic organs including lymph node, thymus, and spleen. The delivery of drugs and bioactive compounds via the lymphatic system is dependent on the physiology of the system. The lymphatic system is able to avoid first-pass metabolism, thus the lymphatic system is suitable for compounds with lower bioavailability, i.e., those undergoing more hepatic metabolism. The lymphatic route also provides an option for the delivery of drugs to treat cancer and human immunodeficiency virus, which can travel through the lymphatic system. The lymphatic route plays an important role in transporting extracellular fluid to maintain homeostasis and in transferring immune cells to injury sites. This paper provides a detailed review of novel lipid-based nanoformulations and their lymphatic delivery. The uptake and distribution of lipid-based nanoformulations by the lymphatic system depends on factors such as particle size, surface charge, molecular weight, and hydrophobicity. Nanoparticulate carriers and their lymphatic delivery via different routes, as well as the in vivo and in vitro models used to study drug transport in the lymphatic systems are also discussed.

Keywords: Lymphatic system, Nanoparticulate carriers, Liposomes, Lymphatic capillary.

1. Introduction

The lymphatic system consists of lymph, lymphatic pathways, such as lymphatic capillary, lymphatic vessel, lymphatic duct etc., and some lymphatic organs including lymph node, thymus, and spleen. The major function of the lymphatic system is to maintain the body's water balance to the normal level as blood vessels do [1, 2]. This system plays an important role in helping to defend the tissues against infection by filtering particles from the lymph and by supporting the activities of the lymphocytes, which furnish immunity, or resistance, to the specific disease causing

agents. Also, it is well known that the lymphatic absorption of a drug after intestinal administration provides an advantage over the portal blood route for the possible avoidance of liver pre-systemic metabolism (hepatic first-pass effect). Due to such fundamental functions or characteristics, many attempts have been made to utilize the lymphatic system for the route of drug delivery, which have been reviewed by Muranish [3]. The lymphatic system differs from the vascular system in capillary structure, circulation pattern, and functions. The lymphatic route

is known to be one of the primary pathways for tumor metastasis. Tumor cells that have detached from the tissue or have invaded a lymphatic vessel become trapped in the meshwork of a lymph node. Some metastatic cancers appear to spread almost exclusively via lymphatics, whereas others also spread through the vascular system [4]. Research into lymphatic targeting has recently attracted increasing interest not only for providing a preferential anticancer chemotherapy, but for improving oral absorption of macromolecule drugs, or achieving mucosal immunity. The lymphatic system is the site of many diseases such as metastatic tuberculosis, cancer, and filariasis [5]. The lymphatics, especially lymph nodes, are also one of the secondary lymphoid organs as is the spleen, Peyer's patches and appendix, and as are the sites where immune responses

are initiated [6,7]. thymus-dependent small lymphocytes, large lymphocytes and macrophages present in lymph nodes produce circulation antibodies, and are involved in immunological reactions. The functions of the lymphatics depend on the blood-lymph communications in various tissues and organs. The large molecular complexes and particles that enter the tissue-fluid will generally be taken up by the fine network of lymphatic capillaries. The lymph passes through one or more lymph nodes and is further transported, via efferent vessels, to the great vein at the base of the neck. While blood circulation generally goes to and returns from every tissue via arteries and veins, lymph flow is usually one-way transport which starts from each tissue and is directed towards the central regions such as the thoracic duct (8).

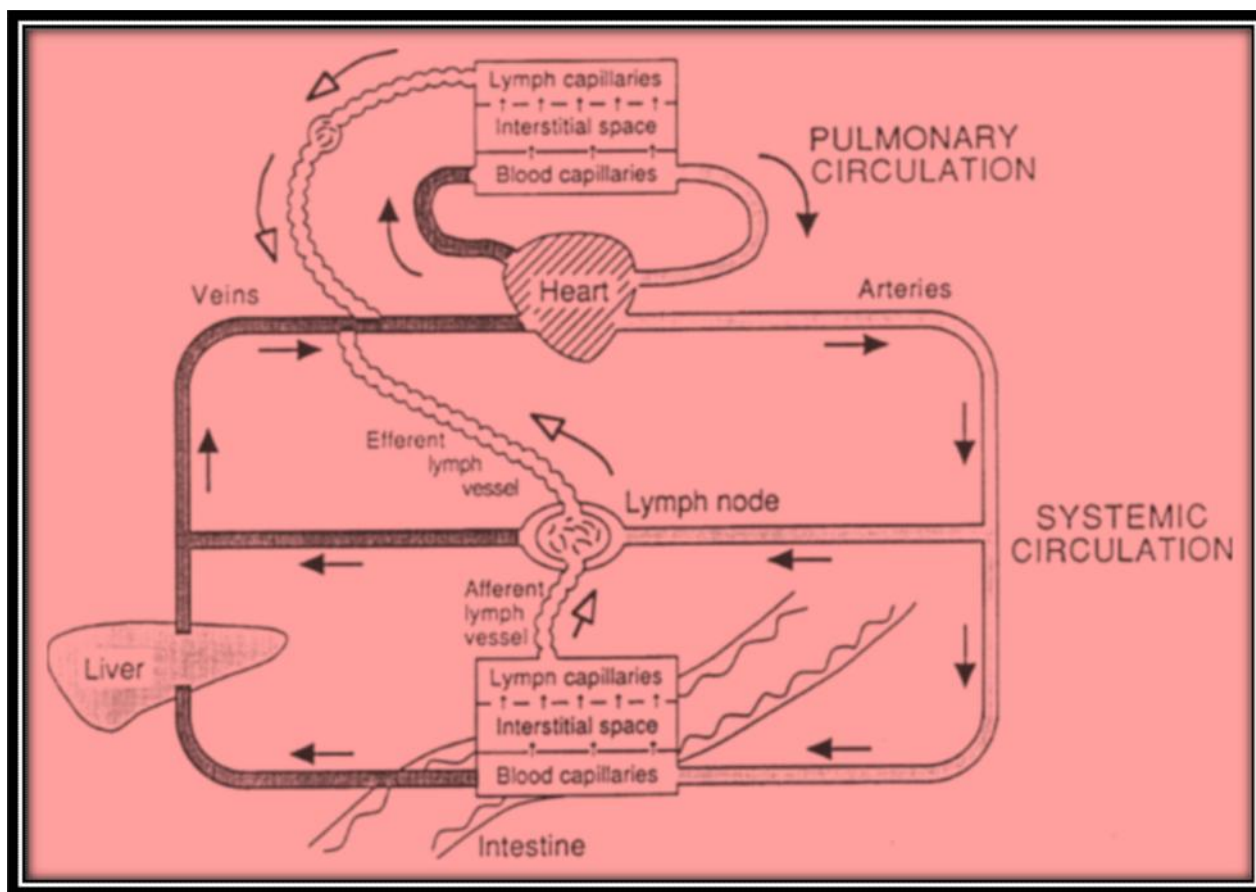


Fig. Lymph- blood communication in body.

2. Effects of carrier systems and administration

A number of water-soluble molecules with a molecular weight of less than 5000 are distributed in equal concentrations between blood and lymph where they do not bind to any endogenous proteins or microparticles: in other words, the concentrations of

smaller molecules do not specifically increase in lymph compared to that in blood fluid. Firstly, if peptide drugs are not large enough, carrier systems such as microparticles or soluble macromolecules of appropriate sizes should be chosen for lympho-selective delivery [8]. Physical complexed binding, incorporation or chemical conjugation to the carrier

system may be applied depending on the properties of the peptide drugs. Secondly, since numerous peptide-degradation enzymes, such as amino-peptidases and endopeptidases, are present in various organs and tissues, strategies for protecting against peptide degradation by various enzymes are usually required [9,10]. Carrier systems may often overcome these obstacles: they can increase the residence time of peptides in the lymph circulation, or can enhance the bioavailability of peptides in the area where they are needed [11,12]. On the other hand, the sites of drug administration considerably influence the lymphatic transport of drugs. For examples, when macromolecules such as dextrans are injected intravenously, an increase in molecular size will decrease the permeability across the blood capillary, and result in a lymph/plasma (LIP) ratio of less than 1 [13,14,15,16]. Under normal tissue conditions, a sufficiently high LIP ratio cannot usually be obtained by intravenous administration. When the small molecules are injected interstitially, about equal concentrations between blood and lymph will be obtained, resulting in a LIP ratio of 1 [17,18,19,20]. Microparticles injected into tissues such as the stomach wall and subcutaneous areas are mainly delivered to lymphatics, resulting in LIP ratios larger than 1 [21,22,23,24]. The reason why the lymph levels become higher than the blood level is that large

molecules penetrate through intracellular gaps of the lymph capillaries despite the difficulty in blood capillary penetration [25,26,27,28,29]. When the macromolecules are administered into a lumen such as the intestine and lung, they have to pass through the mucosal epithelium prior to reaching lymph and blood vessels. The penetration of macromolecules is often tricky: it is difficult for them to pass through the epithelial cells, but for example, pinocytotic uptake in Peyer's patches or penetration through large pores in the alveolar membrane occurs depending on their routes of entry into the body [30,31,32,33,34]. If they can penetrate these barriers, lymphatic uptake of macromolecules or particles would be easily achieved. The gastrointestinal tract is certainly one of the routes for peptide administration [35,36,37]. First, transfer into lymph vessels via absorptive epithelial cells (villous) occurs in two ways: one is the transcellular lipid pathway in which chylomicrons are formed in the cells and transferred into lymph capillaries (Fig. 2a), and the other is the paracellular pathway which usually contributes little, but operates by the addition of absorption enhancers (Fig. 2b) [38,39,40]. The second route is transcytosis through Peyer's patches, and this seems to be most suited for highly potent compounds such as lymphokines and vaccines (Fig. 2c) [41,42].

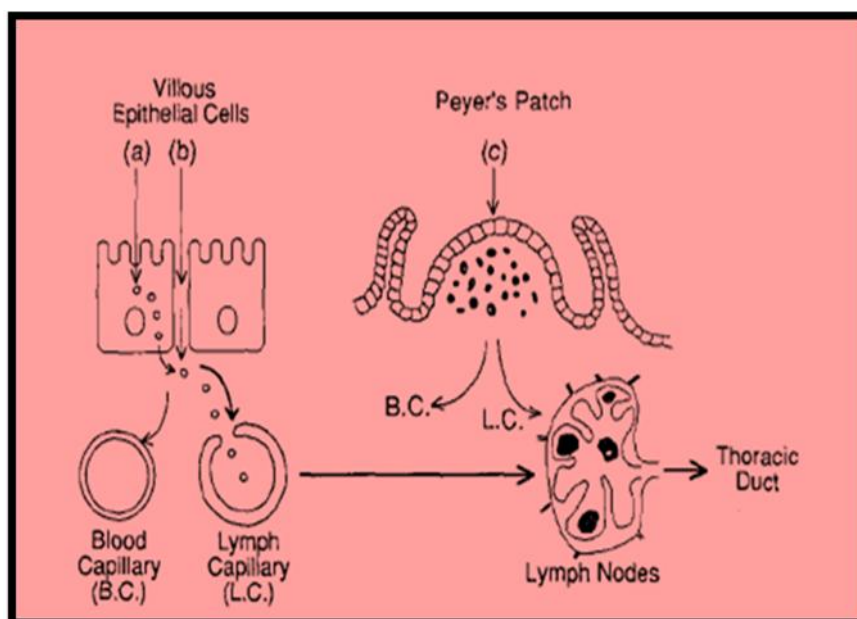


Fig. Lymphatic transfer of drugs via small intestinal epithelial cells and Peyer's patches.

3. Drug –Carriers and drug for lymph targeting⁸.**Table-1**

Lymphotropic carrier	Drug
Carbon colloid	Mitomycinc, aclarubicin
Dextron	Mitomycinc, Adriamycin
L-Lactic acid oligomer microsphere	Aclarubicin, cisplatin
Gelatin microsphere	Mitocin c
-Cyclodextrin oligomer	1-Hexyl-5-fluorouracil
Intrinsic protein complex	Vitamin B12
Styrene-maleic acid anhydride co-polymer	Neocarzinostatin
s/o emulsion	5-fluorouracil, bleomycin
Lipid mixed micelle	Interferon,thf
Chylomicron, LDL	Cyclosporin, vitaminA. Co-enzymeQ
Dextron sulphate	Bleomycin

4. Formulations for lymphatic targeting**Table-2**

Formulations	Drugs	References
Emulsion	Penclomedine	11
Emulsion	Ontazolast	12
Microemulsion	Puerarin	13
Microemulsion	Raloxifene	14
Micellar systems	Cyclosporin A	15
SEEDS	Coenzyme Q10	16
SMEDDS	Halofantrine	17
SMEDDS	Nobiletin	18
SMEDDS	Valsartan	19
SMEDDS	Vinpocetine	20
SMEDDS	Silymarin	21
SMEDDS	Sirolimus	22
SNEDDS	Carvedilol	23
SNEDDS	Valsartan	24
SNEDDS	Halofantrine	25
Liposomes	IgG1	26
Liposomes	Doxorubicin	27–28
Liposomes	Cefotaxime	29
Liposomes	9-nitro-camptothecin	30
Liposomes	Paclitaxel	31
Liposomes	Ovalbumin	32
SLNs	Etoposide	33
SLNs	Methotrexate	34
SLNs	Idarubicin	35
SLNs	Tobramycin	36,37
SLNs	Nimodipine	38
NLCs	Testosterone	39
NLCs	Vinpocetine	40
NLCs	Tripterine	41

5. Nanoparticulate carriers for lymphatic delivery

5.1. Emulsions

Preferential lymphatic transport of mitomycin C has been demonstrated following injection of W/O or O/W emulsions via the intraperitoneal and intramuscular routes [43]. It was reported that selective uptake after injection into the regional lymphatics occurred in the order of O/W. W/O. aqueous solution. Hashida et al. [43, 44] developed gelatin spheres in oil (S/O) emulsion for minimizing the instability of the W/O emulsion. The nanoparticle-in-oil emulsion system, containing anti-filarial drug in gelatin nanoparticles, were studied for enhancing lymphatic targeting [45], and it was suggested that this colloidal system holds excellent potential as a lymphotropic carrier system. More recently, an emulsion formulation consisting of an anticancer drug, Pirarubicin, and Lipiodol[®] was developed to treat gastric cancer and metastatic lymph nodes [46].

5.2. Liposomes

Liposome, a nano-sized biodegradable lipid vesicle with aqueous space surrounded by a lipid bilayer, has received considerable interest as a vehicle for drug targeting to the lymphatic system. Earlier studies suggested that liposome-entrapped compounds were selectively transported into lymphatic tissue following intraperitoneal administration [47,49], intramuscular or subcutaneous injection [50,51]. The effect of liposome size was evaluated by intraperitoneal administration of liposomes with 0.72–0.048 μ m in diameter and having identical compositions [48]. Liposome size significantly altered both fractions of lymphatically absorbed drug retained in lymph nodes and drug recovered in the thoracic duct lymph. The largest liposomes were those most retained by the lymph nodes. It is thought that smaller liposomes pass unretarded through the lymph nodes but that larger liposome may be predominantly entrapped by lymph node tissues during physical filtration. Lymphatic uptake of liposomes of various sizes, lipid composition, and surface characteristics were investigated [52,53]. The main factor controlling lymphatic uptake after subcutaneous administration appeared to be liposome size, and small liposomes seemed to be preferred to achieve high lymphatic uptake. The surface charge of liposomes and the route of administration were reported to be important for the lymphatic delivery of drugs [54]. Following lymphatic uptake, liposomes pass through a system of lymphatic vessels and encounter one or more lymph nodes,

where a fraction will be retained. It has been suggested that phagocytosis by macrophages is one of the major mechanisms of uptake of colloidal particles in lymph nodes [55,56]. Reduced lymph node localization of liposomes in macrophage-depleted lymph nodes confirmed that phagocytosis by macrophages plays an important role in lymph node retention of liposomes [57]. To enhance targeting ability, various attempts have been made so far, including immunoliposome [58], PEGylated liposome [59], and galactosylated liposome [60]. One example of clinical application is the endoscopic gastric submucosal injection of liposomal adriamycin, which provided an enhanced lymph node targeting delivery to considerably higher levels than intravenous free adriamycin in patients with gastric cancer [61–63]. As another example, a pilot study of liposomal mitoxantron for breast cancer was reported [64]. Lymphatic targeting is thought useful for diagnostic purposes. A case study is reported using blue violet entrapped in liposomes to localize lymph nodes before surgery [65]. Polymerized liposomes were developed by Langer et al. [66]. The liposomal structure highly stabilized by cross-linking of lipid bilayer allows the oral administration of those carriers to achieve more efficient uptake from Peyer's patch [67].

5.3. Nanoparticles

Biodegradable, polymeric nanoparticulate systems have been developed to enhance the targeting ability to the lymphatic systems or to improve the drug loading and/or the physicochemical stability of other colloidal carriers. A wide range of studies on the preparation of polyalkylcyanoacrylate nanoparticles and their therapeutic applications has been conducted

by the research groups of Puisieux and Couvreur [68,69]. The lymph targeting of polyhexylcyanoacrylate nanoparticles was evaluated after intraperitoneal administration in rats. It was found that these particles were of potential use in treating tumors that metastasize in the peritoneal cavity or via lymphatic pathways [70,71]. They showed that uptake via Peyer's patches or isolated lymphoid follicles of insulin-loaded polyisobutylcyanoacrylate nanocapsule occurred after oral administration, suggesting the possibility of peroral peptide delivery [72]. Davis and Illum have conducted extensive investigations on biodegradable nanospheres with polylactides and poly(lactide-co-glycolide) as carriers for achieving the efficient delivery of drugs and diagnostic agents to the lymphatic system. To enhance lymphatic drainage and

lymphatic node uptake of nanospheres, various methods of surface engineering have been tried, including surface coating with poloxamines or poloxamers [73] and the use of polyethyleneglycols [74]. Besides the drug delivery purpose, Magnetite-Dextran nanoparticles have been investigated for diagnostic use and found potentially useful as contrast agents in magnetic resonance imaging (MRI) [75]. Lipid-based nanospheres should be alternative colloidal carrier systems for lymphatic targeting. The solid lipid nanoparticles (SLN) were developed and evaluated for the lymphatic uptake after intraduodenal administration to rats [76,77]. A liposomal mimetic formulation, a phospholipid dispersion containing dipalmitoyl-phosphatidylcholine (DPPC) and Emulphor, was also developed and found to achieve higher lymphatic uptake of drug compared to conventional DPPC liposomes [78,79]. As other nano-sized drug carriers, activated charcoal particles have been extensively studied for diagnostic purposes and the targeted delivery of anticancer drugs to the regional lymph node [80–82].

6. Models for study of drug transport in the lymphatic system

6.1. In vivo models

In this model cannulation of the mesenteric or thoracic lymphatic ducts is performed in animals to investigate drug transport in the intestinal lymphatic system [83]. In this model drug concentration are directly measurement of in lymph. The procedure cannot be performed on humans because it is an irreversible and invasive surgical process [84]. In this model Small animals like rats, are commonly used, but some larger animals, including sheep, rabbits, dogs and pigs, have also been used [84-92].

Another in vivo model is the lymphatic venous shunt, in which drug concentrations in lymph are measured at fixed time intervals, and lymph is collected over a longer period of time. Further, an indirect method has been used in an oral bioavailability study to evaluate intestinal lymphatic drug transport in both the presence and absence of inhibitors of intestinal chylomicron flow. This method has the advantage of not requiring a surgical procedure, as does the lymphatic duct cannulation model [93–96].

6.2. In vitro models

Various in vitro models can serve as an alternative to in vivo models for studying lymphatic drug transport. In the intestinal permeability model, Caco-2 cells are used to evaluate intracellular lipoprotein-lipid assembly and to examine the effect of lipids and lipidic excipients on incorporation of drug with lipoproteins in lymphatic transport [97–99]. In one in vitro model, Gershkovich and Hoffman described a correlation between the degree of ex vivo incorporation of a drug into chylomicrons and the extent of intestinal lymphatic drug transport [100]. According to a lipolysis model described by Dahan and Hoffman, in vivo drug absorption could be predicted by evaluating drug release from a lipid-based drug delivery system and estimating precipitation of the drug during lipolysis [101]. Holm and Hoest reported an in silico method that established a quantitative relationship between the molecular structure and amount of drug transferred from the intestinal to the lymphatic system [94–96,102].

7. Conclusion

In current scenario liposomes and solid lipid nanoparticles emerges as a new technology to provide better penetration into the lymphatics where residual disease exists. the lymphatic route can be used for delivery of cytotoxic agents and therapeutic molecules with higher first-pass metabolism and lower solubility so method can serve as a bypass route, especially for anticancer and anti-human immunodeficiency virus drugs, both of which target diseases utilizing the lymphatic system. Drugs that are encapsulated in lipid-based nanoformulations, such as NLCs, are better candidates for lymphatic drug delivery.

References

- [1] J.W. Hole, Lymphatic system and immunity, in: 6th Edition, Human Anatomy Physiology, Wm.C. Brown, 1993, 714– 744.
- [2] J.M. Yoffey, F.C. Courtice, Lymphatics, Lymph and the Lymphomeloid Complex, Academic Press, London, 1970.
- [3] S. Muranishi, Drug targeting towards the lymphatics, Adv. Drug Res. 21, 1991, 1–38.
- [4] T. Takahashi, Emulsion and activated carbon in cancer chemotherapy, CRC Crit. Rev. Ther. Drug Carrier Syst. 2, 1985, 245-274.

- [5] J.N. Weinstein, in: B. Chabner (Ed.), *Rational Basis of Chemotherapy*, A.R. Diss, New York, 1983, 441–473.
- [6]. Mestecky and I.R. McGhee, Immunoglobulin A (IgA): molecular and cellular interactions involved in IgA biosynthesis and immune response, *Adv. Immunol.* 40, 1987, 153-245.
- [7] P. Brandtzaeg, Overview of mucosal immune system, in: I. Mestecky and I.R. McGhee (Eds.), *Current Topics in Microbiology and Immunology*, Springer Verlag, Berlin, Vol. 146, 1986, 13-25.
- [8] S. Muranishi, Drug targeting towards the lymphatics, in: B. Testa (Ed.), *Academic Press*, London, *Advances in Drug Research*, Vol. 21, 1991, 1-38.
- [9] I.P.F. Bai and G.L. Amidon, Structural specificity of mucosal-cell transport and metabolism of peptide drugs: implication for oral peptide drug delivery, *Pharm. Res.* 9, 1992, 969-978.
- [10] X.H. Zhou, Overcoming enzymatic and absorption barriers to non-parenterally administered protein and peptide drugs, *J. Control. Release.* 29, 1994, 239-252.
- [11]. Myers RA, Stella VJ. Factors affecting the lymphatic transport of penclomedine (NSC-338720), a lipophilic cytotoxic drug: comparison to DDT and hexachlorobenzene. *Int J Pharm.* 1992; 80: 51–62.
- [12]. Haus DJ, Fogal SE, Ficorilli JV, et al. Lipid-based delivery systems for improving the bioavailability and lymphatic transport of a poorly water-soluble LTB4 inhibitor. *J Pharm Sci.* 1998; 87: 164–169.
- [13]. Wu H, Zhou A, Lu C, Wang L. Examination of lymphatic transport of puerarin in unconscious lymph duct-cannulated rats after administration in microemulsion drug delivery systems. *Eur J Pharm Sci.* 2011; 42: 348–353.
- [14]. Thakkar H, Nangesh J, Parmar M, Patel D. Formulation and characterization of lipid-based drug delivery system of raloxifene-microemulsion and self-microemulsifying drug delivery system. *J Pharm Bioallied Sci.* 2011; 3: 442–448.
- [15]. Takada K, Yoshimura H, Shibata N, et al. Effect of administration route on the selective lymphatic delivery of cyclosporin A by lipid surfactant mixed micelles. *J Pharmacobiodyn.* 1986;9:156–160.
- [16]. Kommuru TR, Gurley B, Khan MA, Reddy IK. Self-emulsifying drug delivery systems (SEDDS) of coenzyme Q10: formulation development and bioavailability assessment. *Int J Pharm.* 2001;212:233–246.
- [17]. Holm R, Porter CJ, Edwards GA, Müllertz A, Kristensen HG, Charman WN. Examination of oral absorption and lymphatic transport of halofantrine in a triple-cannulated canine model after administration in self-microemulsifying drug delivery systems (SMEDDS) containing structured triglycerides. *Eur J Pharm Sci.* 2003; 20: 91–97.
- [18]. Yao J, Lu Y, Zhou JP. Preparation of nobiletin in self-microemulsifying systems and its intestinal permeability in rats. *J Pharm Pharm Sci.* 2008; 11: 22–29.
- [19]. Dixit AR, Rajput SJ, Patel SG. Preparation and bioavailability assessment of SMEDDS containing valsartan. *AAPS PharmSciTech.* 2010; 11: 314–321.
- [20]. Chen Y, Li G, Wu X, et al. Self-microemulsifying drug delivery system (SMEDDS) of vinpocetine: formulation development and in vivo assessment. *Biol Pharm Bull.* 2008; 31: 118–125.
- [21]. Li X, Yuan Q, Huang Y, Zhou Y, Liu Y. Development of silymarin self-microemulsifying drug delivery system with enhanced oral bioavailability. *AAPS PharmSciTech.* 2010; 11: 672–678.
- [22]. Sun M, Zhai X, Xue K, et al. Intestinal absorption and intestinal lymphatic transport of sirolimus from self-microemulsifying drug delivery systems assessed using the single-pass intestinal perfusion (SPIP) technique and a chylomicron flow blocking approach: linear correlation with oral bioavailabilities in rats. *Eur J Pharm Sci.* 2011;43:132–140.
- [23]. Singh B, Khurana L, Bandyopadhyay S, Kapil R, Katare OO. Development of optimized self-nano-emulsifying drug delivery systems (SNEDDS) of carvedilol with enhanced bioavailability potential. *Drug Deliv.* 2011; 18: 599–612.
- [24]. Beg S, Swain S, Singh HP, Patra CN, Rao MB. Development, optimization, and characterization of solid self-nanoemulsifying drug delivery systems of valsartan using porous carriers. *AAPS PharmSciTech.* 2012; 13: 1416–1427.
- [25]. Holm R, Tønsberg H, Jørgensen EB, Abedinpour P, Farsad S, Müllertz A. Influence of bile on the absorption of halofantrine from lipid-based formulations. *Eur J Pharm Biopharm.* 2012;81:281–287.
- [26]. Moghimi SM, Moghimi M. Enhanced lymph node retention of subcutaneously injected IgG1-PEG2000-liposomes through pentameric IgM antibody-mediated vesicular aggregation. *Biochim Biophys Acta.* 2008;1778:51–55.

- [27]. Ling R, Li Y, Yao Q, et al. Lymphatic chemotherapy induces apoptosis in lymph node metastases in a rabbit breast carcinoma model. *J Drug Target*. 2005;13:137–142.
- [28]. Frenkel V, Etherington A, Greene M, et al. Delivery of liposomal doxorubicin (Doxil) in a breast cancer tumor model: investigation of potential enhancement by pulsed-high intensity focused ultrasound exposure. *Acad Radiol*. 2006; 13: 469–479.
- [29]. O'Brien ME, Wigler N, Inbar M, et al. Reduced cardiotoxicity and comparable efficacy in a phase III trial of pegylated liposomal doxorubicin HCl (Caelyx/Doxil) versus conventional doxorubicin for first-line treatment of metastatic breast cancer. *Ann Oncol*. 2004; 15: 440–449.
- [30]. Ling SS, Magosso E, Khan NA, Yuen KH, Barker SA. Enhanced oral bioavailability and intestinal lymphatic transport of a hydrophilic drug using liposomes. *Drug Dev Ind Pharm*. 2006; 32: 335–345.
- [31]. Lawson KA, Anderson K, Snyder RM, et al. Novel vitamin E analogue and 9-nitro-camptothecin administered as liposome aerosols decrease syngeneic mouse mammary tumor burden and inhibit metastasis. *Cancer Chemother Pharmacol*. 2004;54:421–431.
- [32]. Latimer P, Menchaca M, Snyder RM, et al. Aerosol delivery of liposomal formulated paclitaxel and vitamin E analog reduces murine mammary tumor burden and metastases. *Exp Biol Med (Maywood)*. 2009; 234: 1244–1252.
- [33]. Kojima N, Biao L, Nakayama T, Ishii M, Ikehara Y, Tsujimura K. Oligomannose-coated liposomes as a therapeutic antigen-delivery and an adjuvant vehicle for induction of in vivo tumor immunity. *J Control Release*. 2008; 129: 26–32.
- [34]. Harivardhan RL, Sharma RK, Chuttani K, Mishra AK, Murthy RS. Influence of administration route on tumor uptake and biodistribution of etoposide loaded solid lipid nanoparticles in Dalton's lymphoma tumor bearing mice. *J Control Release*. 2005; 105: 185–198.
- [35]. Paliwal R, Rai S, Vaidya B, et al. Effect of lipid core material on characteristics of solid lipid nanoparticles designed for oral lymphatic delivery. *Nanomedicine*. 2009; 5: 184–191.
- [36]. Zara GP, Bargoni A, Cavalli R, Fundarò A, Vighetto D, Gasco MR. Pharmacokinetics and tissue distribution of idarubicin-loaded solid lipid nanoparticles after duodenal administration to rats. *J Pharm Sci*. 2002;91:1324–1333.
- [37]. Cavalli R, Zara GP, Caputo O, Bargoni A, Fundarò A, Gasco MR. Transmucosal transport of tobramycin incorporated in SLN after duodenal administration to rats. Part I – a pharmacokinetic study. *Pharmacol Res*. 2000;42:541–545.
- [38]. Cavalli R, Bargoni A, Podio V, Muntoni E, Zara GP, Gasco MR. Duodenal administration of solid lipid nanoparticles loaded with different percentages of tobramycin. *J Pharm Sci*. 2003; 92: 1085–1094.
- [39]. Chalikwar SS, Belgamwar VS, Talele VR, Surana SJ, Patil MU. Formulation and evaluation of nimodipine-loaded solid lipid nanoparticles delivered via lymphatic transport system. *Colloids Surf B Biointerfaces*. 2012; 97: 109–116.
- [40]. Muchow M, Maincent P, Müller RH, Keck CM. Production and characterization of testosterone undecanoate-loaded NLC for oral bioavailability enhancement. *Drug Dev Ind Pharm*. 2011; 37: 8–14.
- [41]. Zhuang CY, Li N, Wang M, et al. Preparation and characterization of vinpocetine loaded nanostructured lipid carriers (NLC) for improved oral bioavailability. *Int J Pharm*. 2010; 394: 179–185.
- [42]. Zhou L, Chen Y, Zhang Z, He J, Du M, Wu Q. Preparation of tripterine nanostructured lipid carriers and their absorption in rat intestine. *Pharmazie*. 2012; 67:304–310.
- [43]. M. Hashida, M. Egawa, S. Muranishi, H. Sezaki, Role of intra-muscular administration of water-in-oil emulsions as a method for increasing the delivery of anticancer agents to regional lymphatics, *J. Pharmacokin. Biopharm*. 5 (1997) 223–239.
- [44]. M. Hashida, S. Muranishi, H. Sezaki, Evaluation of water in oil and microsphere in oil emulsions as a specific delivery system of 5-fluorouracil into lymphatics, *Chem. Pharm. Bull*. 25 (1977) 2410–2418.
- [45]. J.S. Karajgi, S.P. Vyas, A lymphotropic colloidal carrier system for diethylcarbamazine: preparation and performance evaluation, *J. Microencaps*. 11 (1994) 539–545.
- [46]. K. Yoshimura, M. Nunomura et al., Evaluation of endoscopic pibarubicin-lipiodol emulsion injection therapy for gastric cancer, *Jpn. J. Cancer Chemother*. 23 (1996) 1519–1522.
- [47]. R.J. Parker, E.R. Priester, S.M. Sieber, Comparison of lymphatic uptake, metabolism, excretion and biodistribution of free and liposome entrapped [¹⁴C]cytosine b-Darabinofuranoside following intraperitoneal administration to rats, *Drug Metab. Dispos*. 10 (1982) 40–46.

- [48] K. Hirano, A.C. Hunt, Lymphatic transport of liposome encapsulated agents: effects of liposome size following intraperitoneal administration, *J. Pharm. Sci.* 74 (1985) 915–921.
- [49] R.J. Parker, K.D. Hartman, S.M. Sieber, Lymphatic absorption and tissue disposition of liposome-entrapped [¹⁴C]adriamycin following intraperitoneal administration to rats, *Cancer Res.* 41 (1981) 1311–1317.
- [50] A.J. Jackson, Intramuscular absorption and regional lymphatic uptake of liposome entrapped inulin, *Drug Metab. Dispos.* 9 (1981) 535–540.
- [51] J. Khato, A.A. del Campo, S.M. Sieber, Carrier activity of sonicated small liposomes containing melphalan to regional lymph nodes of rats, *Pharmacology* 26 (1983) 230–240.
- [52] C. Oussoren, J. Zuidema, D.J.A. Crommelin, G. Storm, Lymphatic uptake and biodistribution of liposomes after subcutaneous injection: II. Influence of liposomal size, lipid composition and lipid dose, *Biochim. Biophys. Acta* 1328 (1997) 261–272.
- [53] C. Oussoren, G. Storm, Lymphatic uptake and biodistribution of liposomes after subcutaneous injection: III. Influence of surface modification with poly(ethylenglycol), *Pharm. Res.* 14 (1977) 1479–1484.
- [54] C.K. Kim, J.H. Han, Lymphatic delivery and pharmacokinetics of methotrexate after intramuscular injection of differently charged liposome-entrapped methotrexate to rats, *J. Microencaps.* 12 (1995) 437–446.
- [55] D.T. O'Hagan, N.M. Christy, S.S. Davis, Particulates and lymphatic drug delivery, in: W.N. Charman, V.J. Stella (Eds.), *Lymphatic Transport of Drugs*, CRC Press, Boca Raton, FL, 1992, pp. 279–315.
- [56] M. Velinova, N. Read, C. Kirby, G. Gregoriadis, Morphological observation on the fate of liposomes in the regional lymph nodes after footpad injection into rats, *Biochim. Biophys. Acta* 1299 (1996) 207–215.
- [57] C. Oussoren, M. Velinova, G. Scherphof, J.J. van der Want, N. van Rooijen, G. Storm, Lymphatic uptake and biodistribution of liposomes after subcutaneous injection: IV. Fate of liposomes in regional lymph nodes, *Biochim. Biophys. Acta* 1370 (1998) 259–272.
- [58] C.K. Kim, Y.J. Choi, S.J. Lim, M.G. Lee, S.H. Lee, S.J. Hwang, Lymph node targeting and pharmacokinetics of ³[³H]methotrexate-encapsulated neutral large unilamellar vesicles and immunoliposomes, *Int. J. Pharm.* 98 (1993) 9–18.
- [59] V.P. Torchilin, Immunoliposomes and PEGylated immunoliposomes: possible use for targeted delivery of imaging agents, *Immunomethods* 4 (1994) 244–258.
- [60] C.K. Kim, E.J. Jeong, Enhanced lymph node delivery and immunogenicity of hepatitis B surface antigen entrapped in galactosylated liposomes, *Int. J. Pharm.* 147 (1997) 143–151.
- [61] Y. Akamo, I. Mizuno, T. Yotsuyanagi, T. Ichino, T. Yamamoto, T. Yasui, Endoscopic gastric submucosal injection of liposomal adriamycin targeting regional lymph nodes in patients with gastric cancer, in: *Proceedings of the American Association of Cancer Research, 83 Meeting, 1992*, p. 255.
- [62] Y. Akamo, I. Mizuno, T. Yotsuyanagi et al., Chemotherapy targeting regional lymph nodes by gastric submucosal injection of liposomal adriamycin in patients with gastric cancer, *Jpn. J. Cancer Res.* 85 (1994) 652–658.
- [63] Y. Akamo, I. Mizuno, H. Takeyama, N. Mohri, T. Ueda, T. Shibata, T. Yotsuyanagi, T. Manabe, Chemotherapy targeting regional lymph nodes by gastric submucosal injection of liposomal adriamycin in patients with gastric cancer, *Jpn. J. Cancer Chemother.* 24 (1997) 1712–1714.
- [64] D. Nagel, G. Storm, S. Koehler, H. Schlebush, U. Wagner, D. Krebs, Lymphatic drug targeting with liposomal mitoxantrone for breast cancer — results of a pilot study, *Eur. J. Cancer* 33 (Suppl. 8) (1997) S176.
- [65] B. Pump, P. Hirnle, Preoperative lymph-node staining with liposomes containing patent blue violet. A clinical case report, *J. Pharm. Pharmacol.* 48 (1996) 699–701.
- [66] J. Okada, S. Cohen, R. Langer, In vitro evaluation polymerized liposome as an oral drug delivery system, *Pharm. Res.* 12 (1995) 576–582.
- [67] H. Chen, V. Torchilin, R. Langer, Polymerized liposomes as potential oral vaccine carrier: stability and bioavailability, *J. Control. Release* 42 (1996) 263–272.
- [68] P. Couvreur, L. Roblot-Treupel, M.F. Poupon, F. Brasseur, F. Puisieux, Nanoparticles as microcarriers for anticancer drugs, *Adv. Drug Del. Rev.* 5 (1990) 209–230.
- [69] P. Couvreur, C. Dubernet, F. Puisieux, Controlled drug delivery with nanoparticles: current possibilities and future trends, *Eur. J. Pharm. Biopharm.* 41 (1995) 2–13.
- [70] P. Maincent, C. Amicabile, P. Thouvenot, M. Hoffman, J. Kreuter, P. Couvreur, Targeting of lymph system with ¹⁴Cpolyacrylic nanoparticles, *Arch. Pharm.* 324 (1991) 637.

- [71] P. Maincent, P. Thouvenot, C. Amicabile, M. Hoffman, J. Kreuter, P. Couvreur, Lymphatic targeting of polymeric nanoparticles after intraperitoneal administration in rats, *Pharm. Res.* 9 (1992) 1534–1539.
- [72] C. Damge, C. Mitchel, M. Aprahamian, P. Couvreur, J.P. Devissaguet, Nanocapsules as carriers for oral peptide delivery, *J. Control. Release* 13 (1990) 233–239.
- [73] A.E. Hawley, L. Illum, S.S. Davis, Lymph node localisation of biodegradable nanospheres surface modified with poloxamer and poloxamine block copolymer, *FEBS Lett.* 400 (1997) 319–323.
- [74] A.E. Hawley, L. Illum, S.S. Davis, Preparation of biodegradable, surface engineered PLGA nanospheres with enhanced lymphatic drainage and lymph node uptake, *Pharm. Res.* 14 (1997) 657–661.
- [75] C. Chouly, D. Pouliquen, I. Lucet, J.J. Jeune, P. Jallet, Development of superparamagnetic nanoparticles for MRI: effect of particle size, charge and surface nature on biodistribution, *J. Microencaps.* 13 (1996) 245–255. " J.-S. C. Schwarz, A.
- [76] R.H. Muller, W. Mehnert, Lucks, " Weyhers, C. Freiras, D. "Muhlen, H. Ruhl, Solid lipid nanoparticles (SLN) — an alternative colloidal carrier for controlled drug delivery, *Eur. J.Pharm. Biopharm.* 41 (1995) 62–69.
- [77] A. Bargoni, R. Cavalli, O. Caputo, A. Fundaro, M.R. Gasco, G.P. Zera, Solid lipid nanoparticles in lymph and plasma after duodenal administration to rats, *Pharm. Res.* 15 (1998) 745–750.
- [78] G. Chen, R. Pasricha, D.S.L. Chow, Characterization of liposomal mimetic formulation for lymphotropic delivery, *Pharm. Res.* 12 (Suppl.) (1995) S261.
- [79] G. Chen, J.A. Double, M. Bibby, D.S.L. Chow, Characterization of liposomal mimetic formulations for selective targeting, *Pharm. Res.* 13 (Suppl.) (1996) S161.
- [80] A. Hagiwara, T. Togawa, J. Yamasaki, M. Ohgaki, T. Imanishi, M. Shirasu, C. Sakakura, T. Yamaguchi, K. Sawai, H. Yamagishi, Extensive gastrectomy and carbon-adsorbed mitomycin C for gastric cancer with peritoneal metastases. Case reports of survivors and their implications, *Hepatogastroenterology* 46 (1999) 1673–1677.
- [81] A. Hagiwara, T. Takahashi, K. Sawai, C. Sakakura, M. Shirasu, M. Ohgaki, T. Imanishi, J. Yamasaki, Y. Takemoto, N. Kageyama, Selective drug delivery to peri-tumoral region and regional lymphatics by local injection of aclarubicin adsorbed on activated carbon particles in patients with breast cancer — a pilot study, *Anticancer-Drugs* 8 (1997) 666–670.
- [82] C. Sakakura, T. Takahashi, K. Sawai, A. Hagiwara, M. Ito, S. Shobayashi, S. Sasaki, K. Ozaki, M. Shirasu, Enhancement of therapeutic efficacy of aclarubicin against lymph node metastases using a new dosage form: aclarubicin adsorbed on activated carbon particles, *Anticancer-Drugs* 3 (1992) 233–236.
- [83]. Boyd M, Risovic V, Jull P, Choo E, Wasan KM. A stepwise surgical procedure to investigate the lymphatic transport of lipid-based oral drug formulations: cannulation of the mesenteric and thoracic lymph ducts within the rat. *J Pharmacol Toxicol Methods.* 2004; 49:115–120.
- [84]. Edwards GA, Porter CJ, Caliph SM, Khoo SM, Charman WN. Animal models for the study of intestinal lymphatic drug transport. *Adv Drug Deliv Rev.* 2001; 50:45–60.
- [85]. Onizuka M, Flatebø T, Nicolaysen G. Lymph flow pattern in the intact thoracic duct in sheep. *J Physiol.*1997; 503(Pt 1):223–234.
- [86]. Segrave AM, Mager DE, Charman SA, Edwards GA, Porter CJ. Pharmacokinetics of recombinant human leukemia inhibitory factor in sheep. *J Pharmacol Exp Ther.* 2004; 309:1085–1092.
- [87]. White DG, Story MJ, Barnwell SG. An experimental model for studying the effects of a novel lymphatic drug delivery system for propranolol. *Int J Pharm.* 1991; 69:169–174.
- [88]. Bocci V, Muscettola M, Grasso G, Magyar Z, Naldini A, Szabo G. The lymphatic route. 1. Albumin and hyaluronidase modify the normal distribution of interferon in lymph and plasma. *Experientia.* 1986; 42:432–433.
- [89]. Khoo SM, Edwards GA, Porter CJ, Charman WN. A conscious dog model for assessing the absorption, enterocyte-based metabolism, and intestinal lymphatic transport of halofantrine. *J Pharm Sci.* 2001; 90: 1599–1607.
- [90]. Khoo SM, Shackelford DM, Porter CJ, Edwards GA, Charman WN. Intestinal lymphatic transport of halofantrine occurs after oral administration of a unit-dose lipid-based formulation to fasted dogs. *Pharm Res.* 2003; 20:1460–1465.
- [91]. Lespine A, Chanoit G, Bousquet-Melou A, et al. Contribution of lymphatic transport to the systemic exposure of orally administered moxidectin in conscious lymph duct-cannulated dogs. *Eur J Pharm Sci.* 2006; 27:37–43.
- [92]. Kagan L, Gershkovich P, Mendelman A, Amsili S, Ezov N, Hoffman A. The role of the lymphatic system in subcutaneous absorption of

- macromolecules in the rat model. *Eur J Pharm Biopharm.* 2007; 67: 759–765.
- [93]. Dahan A, Hoffman A. Evaluation of a chylomicron flow blocking approach to investigate the intestinal lymphatic transport of lipophilic drugs. *Eur J Pharm Sci.* 2005;24:381–388.
- [94]. Trevaskis NL, Charman WN, Porter CJ. Lipid-based delivery systems and intestinal lymphatic drug transport: a mechanistic update. *Adv Drug Deliv Rev.* 2008;60:702–716.
- [95]. Yanez JA, Wang SW, Knemeyer IW, Wirth MA, Alton KB. Intestinal lymphatic transport for drug delivery. *Adv Drug Deliv Rev.* 2011; 63: 923–942.
- [96]. O’Driscoll CM. Lipid-based formulations for intestinal lymphatic delivery. *Eur J Pharm Sci.* 2002; 15:405–415.
- [97]. Seeballuck F, Ashford MB, O’Driscoll CM. The effects of Pluronic block copolymers and Cremophor EL on intestinal lipoprotein processing and the potential link with P-glycoprotein in Caco-2 cells. *Pharm Res.* 2003; 20:1085–1092.
- [98]. Seeballuck F, Lawless E, Ashford MB, O’Driscoll CM. Stimulation of triglyceride-rich lipoprotein secretion by polysorbate 80: in vitro and in vivo correlation using Caco-2 cells and a cannulated rat intestinal lymphatic model. *Pharm Res.* 2004; 21:2320–2326.
- [99]. Karpf DM, Holm R, Garafalo C, Levy E, Jacobsen J, Müllertz A. Effect of different surfactants in biorelevant medium on the secretion of a lipophilic compound in lipoproteins using Caco-2 cell culture. *J Pharm Sci.* 2006; 95:45–55.
- [100]. Gershkovich P, Hoffman A. Uptake of lipophilic drugs by plasma derived isolated chylomicrons: linear correlation with intestinal lymphatic bioavailability. *Eur J Pharm Sci.* 2005; 26:394–404.
- [101]. Dahan A, Hoffman A. Rationalizing the selection of oral lipid based drug delivery systems by an in vitro dynamic lipolysis model for improved oral bioavailability of poorly water soluble drugs. *J Control Release.* 2008;129:1–10.
- [102]. Holm R, Hoest J. Successful in silico predicting of intestinal lymphatic transfer. *Int J Pharm.* 2004; 272:189–193.

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